Contents lists available at ScienceDirect

Journal of Magnetic Resonance

journal homepage: www.elsevier.com/locate/jmr

MQ-PGSTE: A new multi-quantum STE-based PGSE NMR sequence

Gang Zheng, Allan M. Torres, William S. Price*

Nanoscale Organisation and Dynamics Group, College of Health and Science, University of Western Sydney, Campbelltown Campus, Locked Bag 1797, Penrith South DC, NSW 1797, Australia

ARTICLE INFO

Article history: Received 23 December 2008 Revised 5 March 2009 Available online 17 March 2009

Keywords: Diffusion Multi-quantum NMR PGSE Stimulated echo

1. Introduction

For the standard Hahn spin-echo and stimulated echo (STE) based pulsed gradient spin-echo (PGSE) sequences [1,2], the normalized spin-echo attenuation is described by

$$E = \exp\left(\gamma_{\rm eff}^2 Dg^2 \delta^2 (\Delta - \delta/3)\right),\tag{1}$$

where γ_{eff} is the effective gyromagnetic ratio, *D* is the translational diffusion coefficient, g is the strength of the applied pulsed magnetic field gradients, δ is the duration of the pulsed gradients and Δ is the diffusion time (i.e., the timescale of the diffusion measurement). To achieve accurate diffusion determinations, a series of PGSE experiments need to be performed and a maximum attenuation of $\ge 70\%$ (i.e., less than 30% of the original signal intensity remaining) is normally required. However, typical high resolution NMR probes have limited gradient strength (e.g., $g_{max} = 0.6 \text{ T m}^{-1}$) and it is therefore challenging to achieve the attenuation required for the diffusion determination on samples containing macromolecules and macromolecular aggregates due to their relatively short transverse and (possibly) longitudinal relaxation times and slow diffusion (e.g., $D < 10^{-11} \text{ m}^2 \text{ s}^{-1}$). For example, for the standard Hahn spin-echo PGSE sequence with δ = 5 ms, Δ = 200 ms, and a typical maximum gradient strength of 0.6 Tm^{-1} , an attenuation of $\sim 70\%$ can be achieved for the diffusing species with $D = 1 \times 10^{-11} \text{ m}^2 \text{ s}^{-1}$; however, many macromolecular aggregates have smaller diffusion coefficients and extremely short transverse relaxation time so it becomes impossible to accurately determine the diffusion of these species without significant signal loss owing to the use of long diffusion

ABSTRACT

A new multi-quantum stimulated echo based pulsed gradient spin-echo sequence, MQ-PGSTE, has been developed for measuring translational diffusion. The new sequence provides a higher signal-to-noise ratio than the (Hahn spin-echo based) MAXY-D sequence at long diffusion times, and thus potentially affords better diffusion measurements on macromolecule samples. Based on multi-quantum coherence encoding, the MQ-PGSTE sequence needs considerably lower gradient strengths for diffusion characterization compared to standard single quantum pulsed gradient spin-echo sequences. By using the new sequence, the diffusion coefficient of L-[3-¹³C]-alanine was found to be 8.1 ± 0.1 × 10⁻¹⁰ m² s⁻¹, which is in line with the value obtained by the use of the standard stimulated echo based pulsed gradient spin-echo sequence.

© 2009 Elsevier Inc. All rights reserved.

times. It is desirable therefore to develop new methods that facilitate diffusion measurements on these slowly diffusing species.

Based on the attenuation term with the effective gyromagnetic ratio (i.e., Eq. (1)), there are two common ways to increase the attenuation for the same gradient parameters by manipulating spins: (i) Enhancing γ_{eff} by using multi-quantum (MQ) coherences (e.g., [3,4]) (e.g., $\gamma_{\text{eff}} = 3 \gamma_{1\text{H}} + \gamma_{13\text{C}}$ for the quadruple quantum (QQ) coherence of $8^{1}\text{H}_{x}^{-1}\text{H}_{y}^{-1}\text{H}_{y}^{-13}\text{C}_{x}$ while $\gamma_{\text{eff}} = \gamma_{1\text{H}}$ for $^{1}\text{H}_{x}$); (ii) Using long T_{1} species (e.g., $^{15}\text{N}_{z}$) in STE-based PGSE experiments to extend Δ (e.g., [5]). In this study, we focus on the enhancement of γ_{eff} by the use of heteronuclear MQ coherences.

Homonuclear MQ PGSE experiments were first developed in the 1980's for the study of anisotropic diffusion in various liquid crystals due to their abilities to enhance γ_{eff} and remove dipolar couplings [6,7]. Whereas, heteronuclear MQ PGSE experiments were mainly developed for the selection of ${}^{1}\text{H}{-}{}^{15}\text{N}$ MQ coherences in the diffusion measurements on proteins (e.g., [8,9]).

The core parts of the heteronuclear MQ PGSE sequences are the MQ coherence generation units. One of the simplest and most effective MQ coherence generation units is the maximum-quantum proton spectroscopy (MAXY) unit [10], 90_x° (I) – $1/(2 J_{IS})$ – 180_x° (I) 90_x° (S) – $1/(2 J_{IS})$ – 90_x° (I), which is a modified version of the DEPT [11] sequence, where I stands for ¹H, S stands for ¹³C, and J_{IS} is the ¹³C–¹H J-coupling constant. The evolution of product operators for SI_n (where n = 1 for ¹³C¹H, n = 2 for ¹³C¹H₂, and n = 3 for ¹³C¹H₃) during the MAXY unit is [10]

$$SI_{n} :+ I_{z} \xrightarrow{90_{s}^{*}(I)} - I_{y} \xrightarrow{\pi J_{B}\tau(2I_{z}S_{z})} + 2I_{x}S_{z} \xrightarrow{180_{s}^{*}(I)90_{s}^{*}(S)} - 2I_{x}S_{y}$$

$$\xrightarrow{\pi J_{B}\tau(2I_{z}S_{z})} - 2I_{x}S_{y} \xrightarrow{90_{s}^{*}(I)} - 2I_{x}S_{y} \qquad n = 1$$

$$+ 4I_{x}I_{z}S_{x} \qquad - 4I_{x}I_{y}S_{x} \qquad n = 2$$

$$+ 8I_{x}I_{z}I_{z}S_{y} \qquad + 8I_{x}I_{y}I_{y}S_{y} \qquad n = 3.$$

$$(2)$$



^{*} Corresponding author. Fax: +61 2 4620 3025.

E-mail address: w.price@uws.edu.au (W.S. Price).

^{1090-7807/\$ -} see front matter @ 2009 Elsevier Inc. All rights reserved. doi:10.1016/j.jmr.2009.03.004

As shown in Scheme (2), the MAXY unit generates the maximum-quantum coherences (i.e., double quantum (DQ) coherence of ${}^{13}C^{1}H$, triple quantum (TQ) coherence of ${}^{13}C^{1}H_{2}$, and QQ coherence of ${}^{13}C^{1}H_{3}$) and therefore the maximum enhancement of γ_{eff} .

By combining the MAXY unit with the standard Hahn spin-echo based PGSE sequence, Liu et al. [12] and Luo et al. [13] developed the MAXY-D sequence (Fig. 1A) for MQ PGSE experiments. However, because the MAXY-D sequence is based on the Hahn spinecho sequence [14], it suffers significant signal loss caused by transverse relaxation when long diffusion times (e.g., 500 ms) are employed. In order to minimize the signal loss due to transverse relaxation, which is normally very significant in the diffusion measurements of macromolecules and macromolecular aggregates, an STE-based equivalent of the MAXY-D sequence, MQ-PGSTE (Fig. 1B), was developed by combining the MAXY unit with the standard STE-based PGSE sequence. The new sequence was tested on a sample containing L-[3-¹³C]-alanine.

2. Materials and methods

L-[3-¹³C]-alanine (ISOTEC, Matheson, Miamisburg) 4.3 mg was dissolved in 5 mL ²H₂O (ISOTEC, Matheson, Miamisburg) to give a 9.6 mM L-[3-¹³C]-alanine solution. 0.3 ml of this solution was dispensed into a magnetic susceptibility-matched (to ²H₂O) NMR tube (BMS-003, Shigemi, Tokyo).

¹H PGSE NMR spectra were acquired on a Bruker Avance 500 spectrometer (Karlsruhe, Germany) at 500 MHz using a TXI high



Fig. 2. The ¹H MAXY-D L-[3-¹³C]-alanine spectra with Δ = 50 ms (A) and 500 ms (B) and the ¹H MQ-PGSTE L-[3-¹³C]-alanine spectra with Δ = 50 ms (C) and 500 ms (D). g_1 = 0.007 T m⁻¹, g_3/g_2 = 13/4 for selecting the QQ coherence from ¹³C¹H₃, and number-of-scans = 64.

resolution probe equipped with a gradient coil at 25 °C. ¹³C CW decoupling was used during acquisition. Typical acquisition parameters were: spectral width 7 kHz; digitized into 20 K data points; $\pi/2$ pulse length 8–9 µs for ¹H and 19–20 µs for ¹³C. Diffusion measurements were performed by linearly incrementing g_1 from 0.02 to 0.22 T m⁻¹.



Fig. 1. The MAXY-D (A) and MQ-PGSTE (B) sequences. Black bars, hollow bars, and grey rectangles represent $\pi/2$, π , and gradient pulses, respectively; g_1 is used for diffusion determination and g_2 and g_3 are used for MQ coherence selection with $g_3/g_2 = (\gamma_{13C} + 3 \gamma_{1H})/\gamma_{1H} = 13/4$ for ${}^{13}C^{1}H_3$, $g_3/g_2 = (\gamma_{13C} + 2 \gamma_{1H})/\gamma_{1H} = 9/4$ for ${}^{13}C^{1}H_2$, and $g_3/g_2 = (\gamma_{13C} + 3 \gamma_{1H})/\gamma_{1H} = 5/4$ for ${}^{13}C^{1}H$, $\tau = 1/(2 J_{13C})$ and τ' is long enough to let eddy currents dissipate. For the MAXY-D sequence, $\phi_1 = x$, -x, $\phi_2 = x$, x, -x, and $\phi_r = -y$, y, y, -y: for the MQ-PGSTE sequence, $\phi_1 = x$, -x, $\phi_2 = x$, x, -x, -x, and $\phi_r = -y$, y, y, -y.



Fig. 3. The ¹H MQ-PGSTE 1-[3-¹³C]-alanine spectra with Δ = 30 ms, g_3/g_2 = 13/4, number-of-scans = 16, and different g_1 values. The diffusion decays calculated from the spectra presented are also shown. A small residual HDO signal is evident in some of the spectra and is likely the result of imperfect coherence selection.

Maple 12 (Maplesoft, Waterloo) was used for the Stejskal and Tanner analysis [1] of the new sequence. Origin 8 (OriginLab, Northampton, MA) was used for all diffusion data analysis.

3. Results and discussion

For the MQ-PGSTE sequence (Fig. 1B), the evolution of the product operators [15] after the MAXY unit may be written as

$$\begin{split} SI_{1} &:= 2I_{x}S_{y} \qquad \xrightarrow{g_{1}-180_{y}^{o}(I)180_{x}^{o}(S)-g_{1}} \rightarrow -2I_{x}S_{y} \qquad \xrightarrow{90_{x}^{o}(I)} \rightarrow -2I_{x}S_{y} \\ SI_{2} &:= -4I_{x}I_{y}S_{x} \qquad +4I_{x}I_{y}S_{x} \qquad +4I_{x}I_{z}S_{x} \\ SI_{3} &:+ 8I_{x}I_{y}I_{y}S_{y} \qquad +8I_{x}I_{y}I_{y}S_{y} \qquad +8I_{x}I_{z}I_{z}S_{y} \\ \xrightarrow{\pi J_{15}\tau(2I_{z}S_{z})} \rightarrow \xrightarrow{180_{x}^{o}(I)90_{x}^{o}(S)} \rightarrow \xrightarrow{\pi J_{B}\tau(2I_{z}S_{z})} \rightarrow \xrightarrow{90_{x}^{o}(I)} \rightarrow -I_{z} \xrightarrow{90_{x}^{o}(I)} \rightarrow +I_{y} \\ &+ I_{z} \qquad -I_{y} \\ -I_{z} \qquad +I_{y} \\ \xrightarrow{\pi J_{15}\tau(2I_{z}S_{z})} \rightarrow \xrightarrow{180_{x}^{o}(I)90_{x}^{o}(S)} \rightarrow \xrightarrow{\pi J_{B}\tau(2I_{z}S_{z})} \xrightarrow{90_{x}^{o}(I)} \rightarrow +2I_{x}S_{y} \\ &-8I_{x}I_{y}I_{y}S_{y} \\ \xrightarrow{g_{1}-180_{x}^{o}(I)180_{x}^{o}(S)-g_{1}-g_{z}} \rightarrow \xrightarrow{90_{x}^{o}(I)-\pi J_{15}\tau(2I_{z}S_{z})-180_{x}^{o}(I)90_{x}^{o}(S)-\pi J_{B}\tau(2I_{z}S_{z})-g_{3}} \rightarrow +I_{y} \\ &+I_{y} \\ \end{split}$$

$$(3)$$

As shown in Scheme (3), MQ terms are generated after the application of the MAXY unit. The $8I_xI_yI_yS_y$ term is dephased by the application of g_1 gradients and only one of the dephased MQ terms is selected and transformed into I_z , which is not susceptible to transverse relaxation, by the use of another MAXY unit, that is the MQ-to-SQ transformation of the dephased MQ term causes signal loss. After the storage period (i.e., τ_2 period), I_z is transformed into dephased $8I_xI_yI_yS_y$, rephased by the application of g_1 gradients, and then transformed into (measurable) I_y .

To demonstrate the *S*/*N* ratio enhancement of the MQ-PGSTE sequence, the MAXY-D and MQ-PGSTE experiments were performed with a relatively short diffusion time (i.e., 50 ms) and a relatively long diffusion time (i.e., 500 ms) (Fig. 2). As shown in Fig. 2A and

Fig. 2C, at short diffusion times, the MQ-PGSTE sequence provided a lower *S*/*N* ratio than the MAXY-D sequence due to the signal loss by using a stimulated echo and more MQ-to-SQ transformations; as shown in Fig. 2B and D, however, at long diffusion times, the MQ-PGSTE sequence provided a much higher *S*/*N* ratio than the MAXY-D sequence due to its much lower susceptibility to transverse relaxation. Therefore, the MQ-PGSTE sequence is preferable for studying macromolecules and macromolecular aggregates, which usually have very short transverse relaxation times. Furthermore, the HDO resonance at 4.8 ppm was completely removed, indicating that the new sequence affords solvent suppression.

The echo attenuation for the MQ-PGSTE sequence can be described by

$$E = \exp\left(-\frac{2}{3}\gamma_{\rm eff}^2 g_1^2 \delta^2 D(6\Delta - 3\tau' - \delta)\right),\tag{4}$$

where $\gamma_{eff} = \gamma_{1_H} + \gamma_{1_3_C}$, 2 $\gamma_{1_H} + \gamma_{1_3_C}$, and 3 $\gamma_{1_H} + \gamma_{1_3_C}$ for ${}^{1_3}C^1H$, ${}^{1_3}C^1H_2$, and ${}^{1_3}C^1H_3$, respectively.

A MQ-PGSTE diffusion experiment was performed on the L-[3-¹³C]-alanine sample (Fig. 3) and the obtained diffusion coefficient (i.e., $8.1 \pm 0.1 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$) is in line with the diffusion coefficient ($7.9 \pm 0.1 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$) measured using the standard STE-based PGSE sequence.

4. Conclusions

Due to its lower susceptibility to transverse relaxation, the MQ-PGSTE sequence provides a higher signal-to-noise ratio than the MAXY-D sequence at long diffusion times, and is thus suitable for better diffusion measurements on macromolecule samples. However, both MQ-PGSTE and MAXY-D sequences suffer from significant signal loss due to the MQ-to-SQ transformations of the dephased MQ coherences. We are currently investigating improved MQ-to-SQ transformation strategies.

Acknowledgments

This research was supported by an Endeavour International Postgraduate Research Scholarship from the University Western Sydney and the Australian Government (G.Z.), and a NSW BioFirst Award from the NSW Ministry for Science & Medical Research (W.S.P.).

References

- E.O. Stejskal, J.E. Tanner, Spin diffusion measurements: spin echoes in the presence of a time-dependent field gradient, J. Chem. Phys. 42 (1965) 288–292.
- [2] J.E. Tanner, Use of the stimulated echo in NMR diffusion studies, J. Chem. Phys. 52 (1970) 2523–2526.
- [3] S. Vega, A. Pines, Operator formalism for double quantum NMR, J. Chem. Phys. 66 (1977) 5624–5644.
- [4] A. Wokaun, R.R. Ernst, The use of multiple quantum transitions for relaxation studies in coupled spin systems, Mol. Phys. 36 (1978) 317-341.
- [5] F. Ferrage, M. Zoonens, D.E. Warschawski, J.-L. Popot, G. Bodenhausen, Slow diffusion of macromolecular assemblies by a new pulsed field gradient NMR method, J. Am. Chem. Soc. 125 (2003) 2541-2545 (Also see Erratum to document cited in CA138:250938, J. Am. Chem. Soc. 126 (2004) 5654).
- [6] J.F. Martin, L.S. Selwyn, R.R. Vold, R.L. Vold, The determination of translational diffusion constants in liquid crystals from pulsed field gradient double quantum spin echo decays, J. Chem. Phys. 76 (1982) 2632–2634.
- [7] D. Zax, A. Pines, Study of anisotropic diffusion of oriented molecules by multiple quantum spin echoes, J. Chem. Phys. 78 (1983) 6333–6334.

- [8] M.L. Tillett, M.A. Horsfield, L.-Y. Lian, T.J. Norwood, Protein-ligand interactions measured by ¹⁵N-filtered diffusion experiments, J. Biomol. NMR 13 (1999) 223–232.
- [9] A.J. Dingley, J.P. Mackay, G.L. Shaw, B.D. Hambly, G.F. King, Measuring macromolecular diffusion using heteronuclear multiple-quantum pulsedfield-gradient NMR, J. Biomol. NMR 10 (1997) 1–8.
- [10] M. Liu, D. Farrant, J.K. Nicholson, J.C. Lindon, Selective detection of ¹H NMR resonances of CH_n groups using a heteronuclear maximum-quantum filter and pulsed field gradients, J. Magn. Reson. B 106 (1995) 270–278.
- [11] D.M. Doddrell, D.T. Pegg, M.R. Bendall, Distortionless enhancement of NMR signals by polarization transfer, J. Magn. Reson. 48 (1982) 323–327.
- [12] M.L. Liu, X.A. Mao, C.H. Ye, J.K. Nicholson, J.C. Lindon, Enhanced effect of magnetic field gradients using multiple quantum NMR spectroscopy applied to self-diffusion coefficient measurement, Mol. Phys. 93 (1998) 913–920.
- [13] R.S. Luo, M.L. Liu, X.A. Mao, Eliminating systematic error in multiple quantum diffusion measurements by bipolar gradient pulses, Meas. Sci. Technol. 9 (1998) 1347–1350.
- [14] E.L. Hahn, Spin echoes, Phys. Rev. 80 (1950) 580-594.
- [15] O.W. Sørensen, G.W. Eich, M.H. Levitt, G. Bodenhausen, R.R. Ernst, Product operator formalism for the description of NMR pulse experiments, Prog. Nucl. Magn. Reson. Spectrosc. 16 (1983) 163–192.